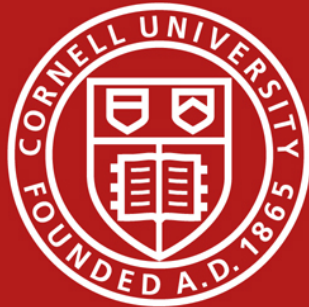


# Multiscale model of platelet adhesion and thrombus formation: validation with the humanized mouse



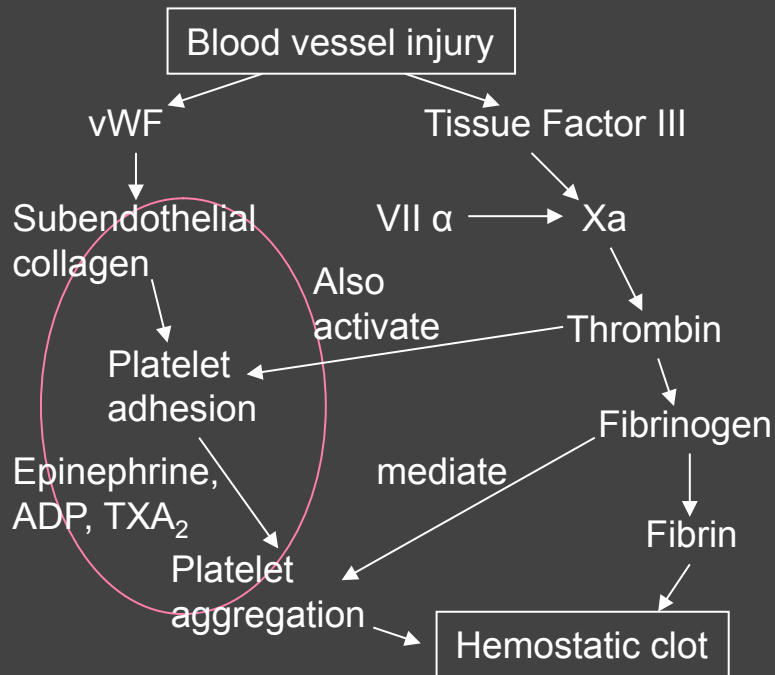
Cornell University

Weiwei Wang<sup>1</sup>, John P. Lindsey II<sup>1</sup>, Jianchun Chen<sup>2</sup>,  
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1. Department of Biomedical Engineering, Cornell University,  
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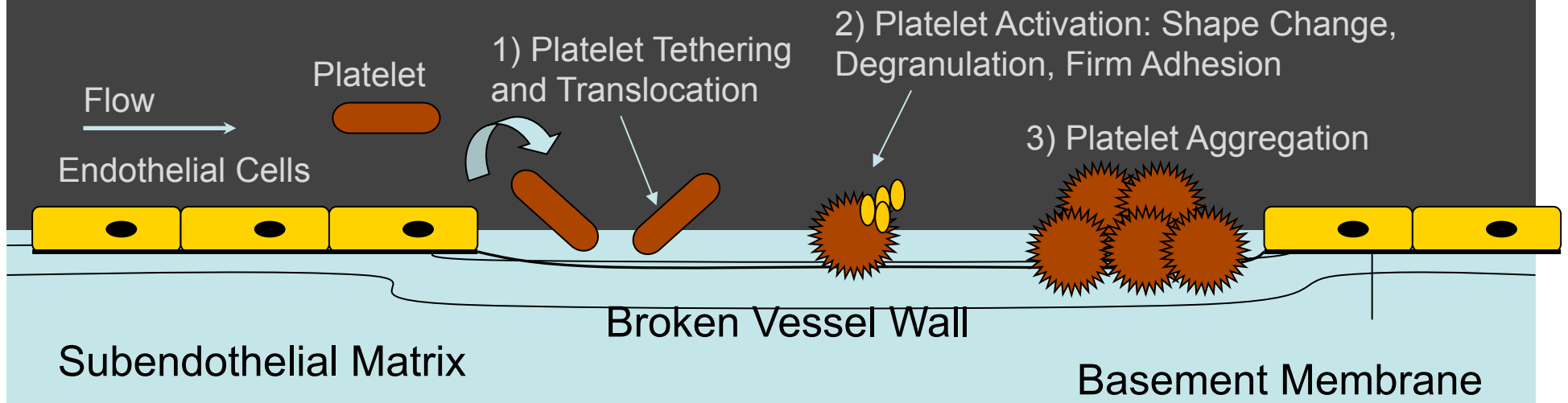
3. Departments of Mechanical Science & Engineering and  
Aerospace Engineering, University of Illinois at Urbana-  
Champaign, Urbana, IL 61801, USA

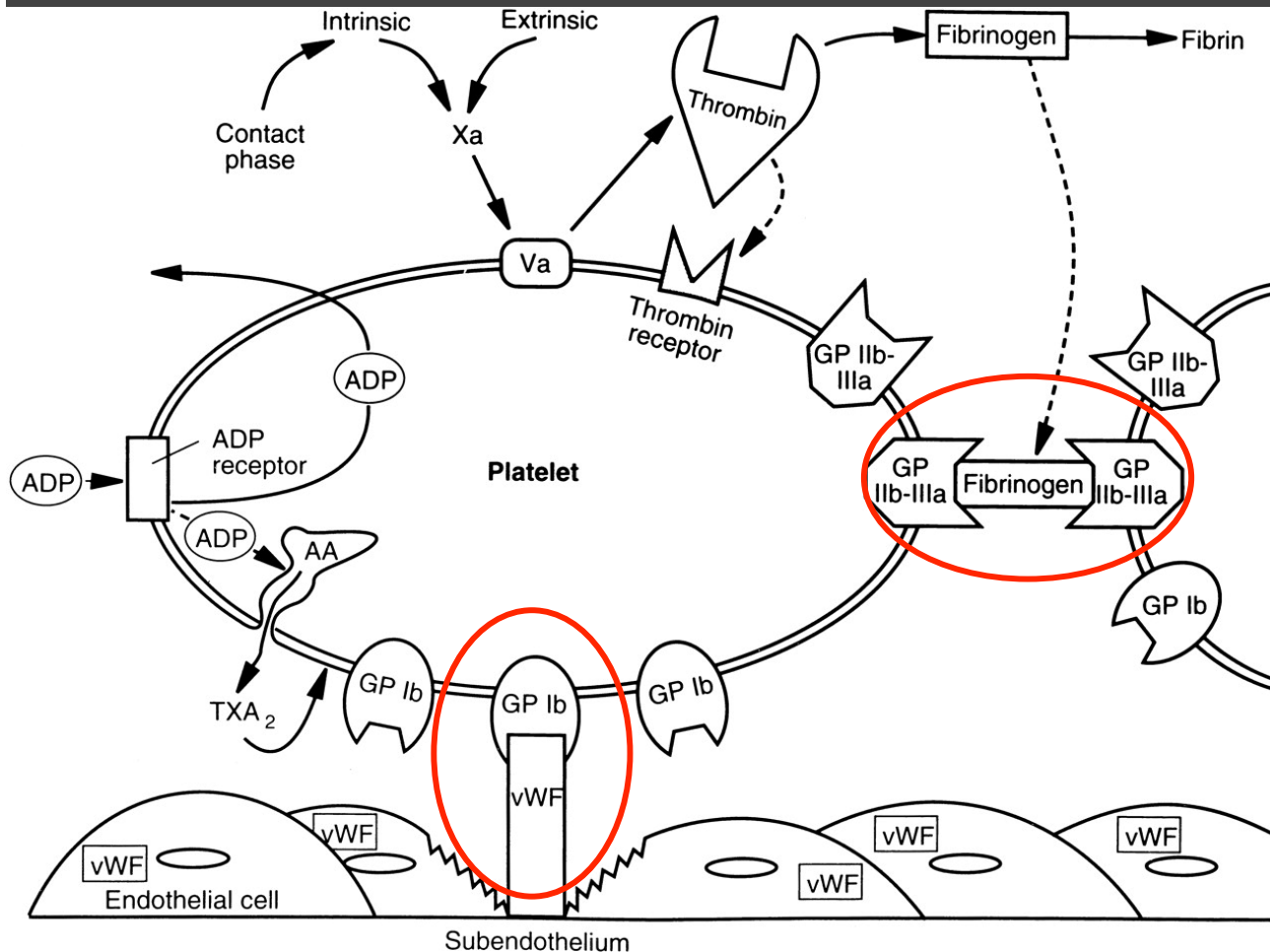


• **Hemostasis** describes the physiological process of blood clotting at injured vessels

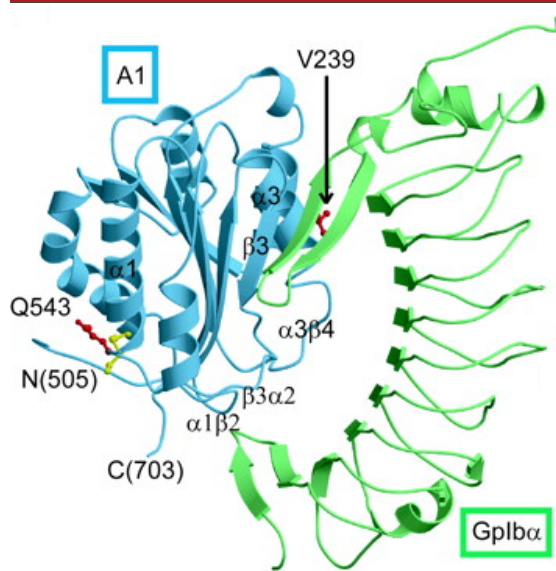
• **Thrombosis** involves platelet activation and aggregation under pathological conditions

The **left** pathway reacts much **faster** than the right pathway, which makes **platelet** a key component in the initiation of hemostasis.





Our research utilizes computational simulation models to study the adhesion of flowing platelets onto injured vessel surfaces, the initiation of thrombosis and the further development of micro-thrombi mediated by GPIb, integrin  $\alpha 2\beta 1$ , GP IIb/IIIa receptors.



“GPIb-vWF-A1 tether bond kinetics are “selectin-like”:

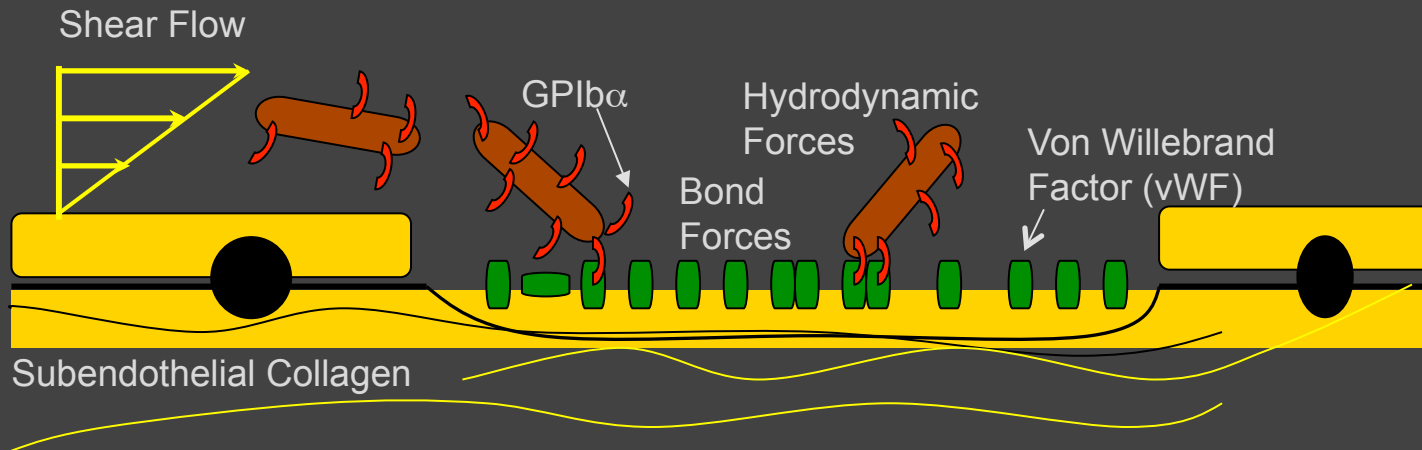
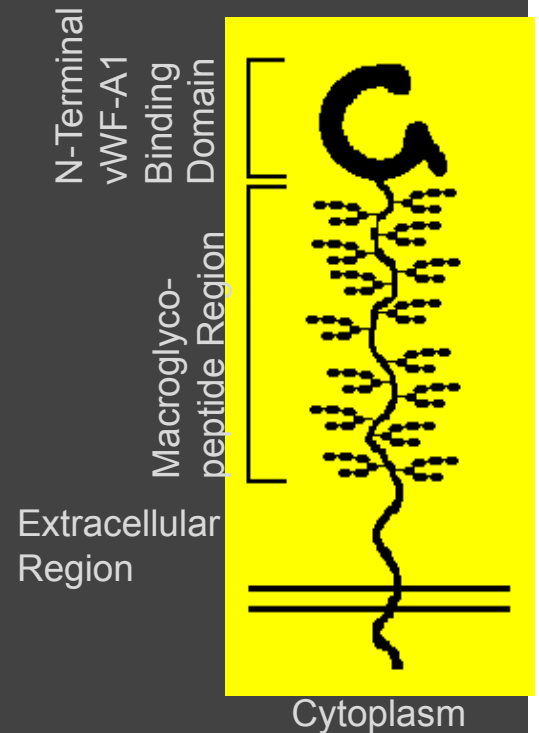
- 1) a critical level of hydrodynamic flow to initiate adhesion
- 2) short-lived tethering events
- 3) fast intrinsic dissociation rate constant.”

--TA Doggett, et al.

EG. Huizinga, et al. Science 16 August 2002: Vol. 297 no. 5584 pp. 1176-1179

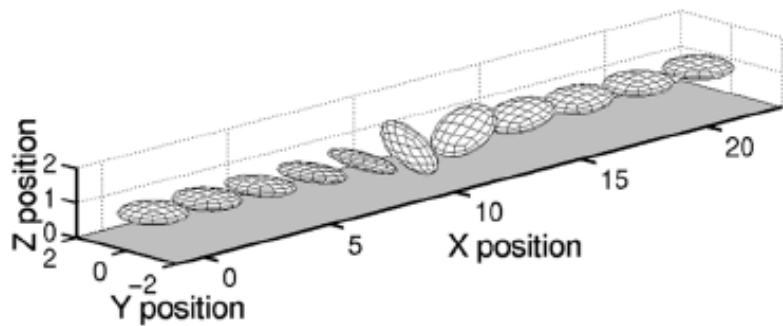
TA Doggett, et al. Biophysical Journal Volume 83 July 2002 194–205

GPIba Structure





# Convective Transport of a Single Platelet



Nipa Mody, et al. Phys. Fluids, 2005

One solid near-wall spheroid convects under simple shear Stoke's flow.

Governing equations:

$$\nabla p = \mu \nabla^2 u, \quad \nabla \cdot v = 0 \quad u_\infty = \gamma z$$

$$\mathbf{u} = \mathbf{U}^{(p)} + \boldsymbol{\omega}^{(p)} \times (\mathbf{x} - \mathbf{x}^{(p)}) \quad \mathbf{x} \in S^{(p)},$$

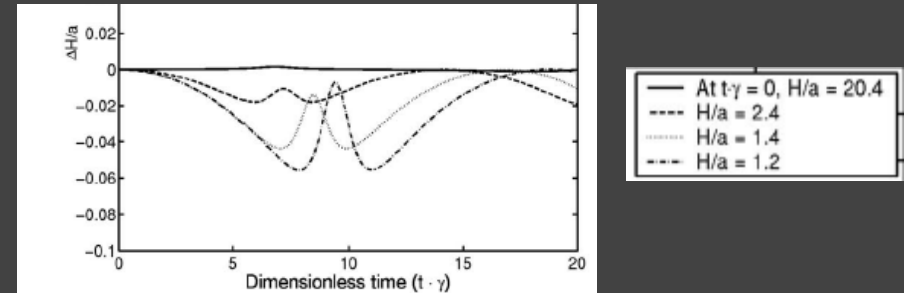
CDL-BIEM method (a boundary integral method to solve Stoke's flow):

$$\mathbf{v}(\mathbf{x}) - \mathbf{v}^\infty(\mathbf{x}) = \mathbf{v}^{RC}(\mathbf{x}) + \oint_S \mathbf{K}(\mathbf{x} - \boldsymbol{\xi}) \cdot \boldsymbol{\phi}(\boldsymbol{\xi}) dS(\boldsymbol{\xi})$$

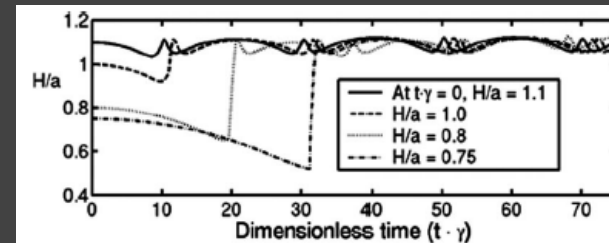
$$\mathbf{K}(\mathbf{x} - \boldsymbol{\xi}) = -2\mathbf{n}(\boldsymbol{\xi}) \cdot \boldsymbol{\Sigma}(\mathbf{x} - \boldsymbol{\xi}) \quad \boldsymbol{\Sigma}(\mathbf{x}) = -\frac{3}{4\pi} \mathbf{x}\mathbf{x}\mathbf{x}/|\mathbf{x}|^5$$

$$\mathbf{v}^{RC}(\mathbf{x}) = \sum_{\alpha=1}^N [\mathbf{F}_\alpha^e - \frac{1}{2}(\mathbf{T}_\alpha^e \times \nabla)] \cdot \frac{\mathcal{G}(\mathbf{x} - \mathbf{x}_\alpha)}{8\pi\mu} \quad \frac{\mathcal{G}_{ij}(\mathbf{x})}{8\pi\mu} = \frac{1}{|\mathbf{x}|} \delta_{ij} + \frac{1}{|\mathbf{x}|^3} x_i x_j$$

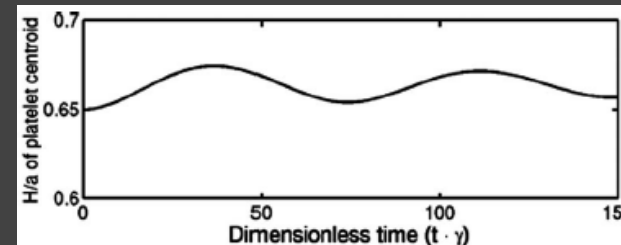
**Regime 1:** Modified Jeffery orbit. ( $H > 1.2a$ )  
 $H$ : start height,  $a$ : platelet long axis length



**Regime 2:** "Pole-vaulting" followed by repeated contacting. ( $1.1a > H > 0.75a$ )

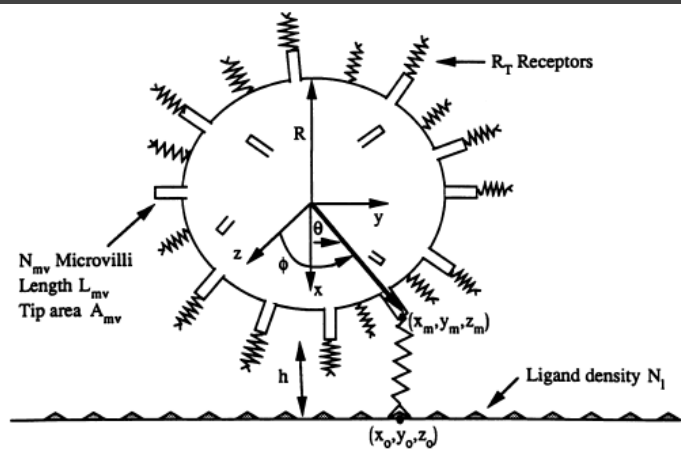


**Regime 3:** Wobble flow. ( $H < 0.70a$ )





Prototype—  
Selectin mediated neutrophil rolling:



DA Hammer, et al. Biophys. J. Volume 63 July 1992 35-57

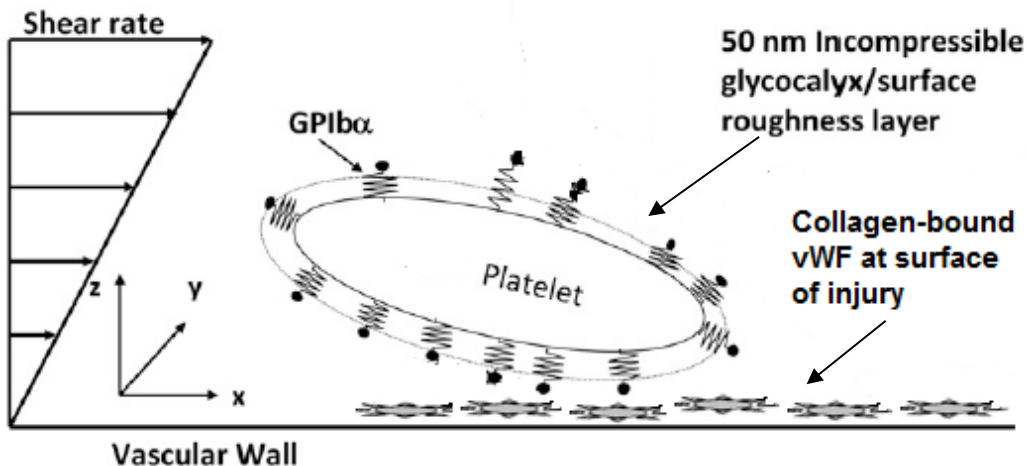
Bond kinetics, based on Bell Model:

$$P_f = 1 - \exp(-k_f \Delta t)$$

$$P_r = 1 - \exp(-k_r \Delta t)$$

$$k_r = k_r^0 \exp\left(\frac{\gamma F_b}{k_B T}\right)$$

$$k_f = k_{f,2-D}^0 \exp\left(\sigma |x_b - l_b| \frac{\gamma - 0.5|x_b - l_b|}{k_b T}\right)$$

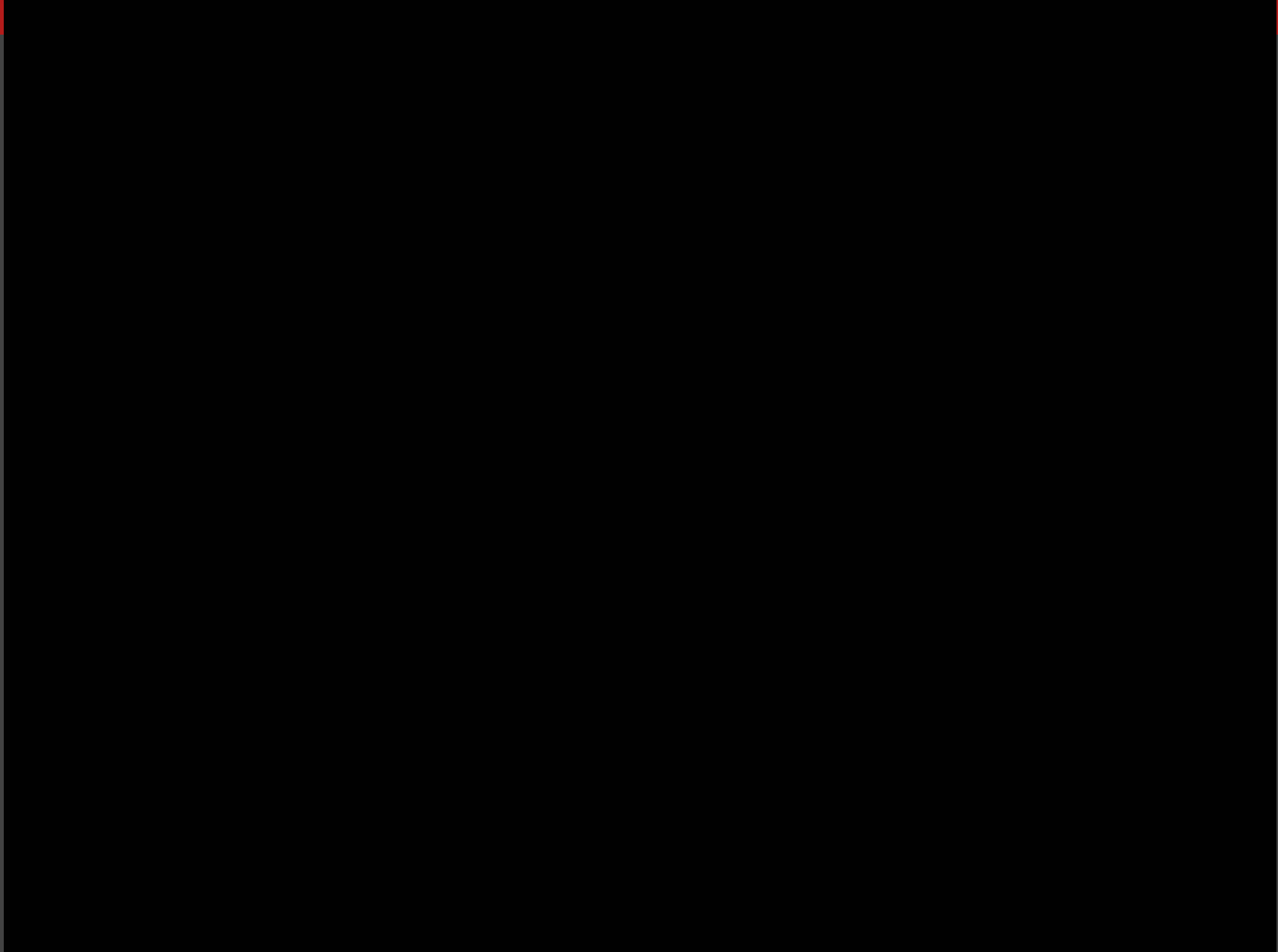


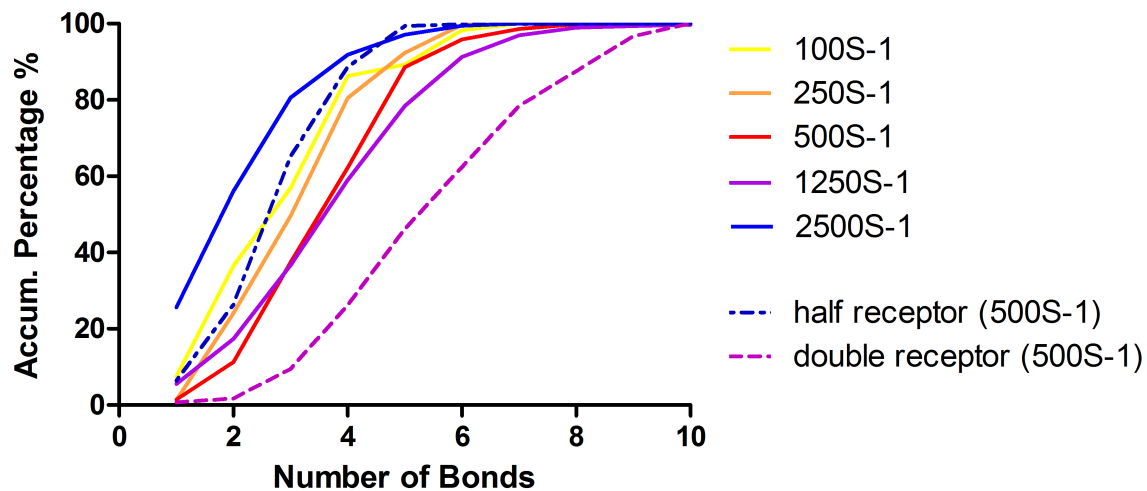
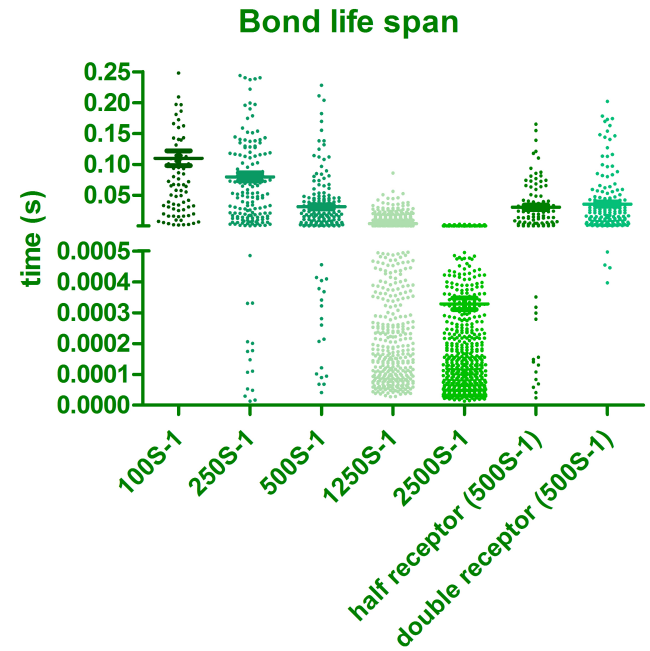
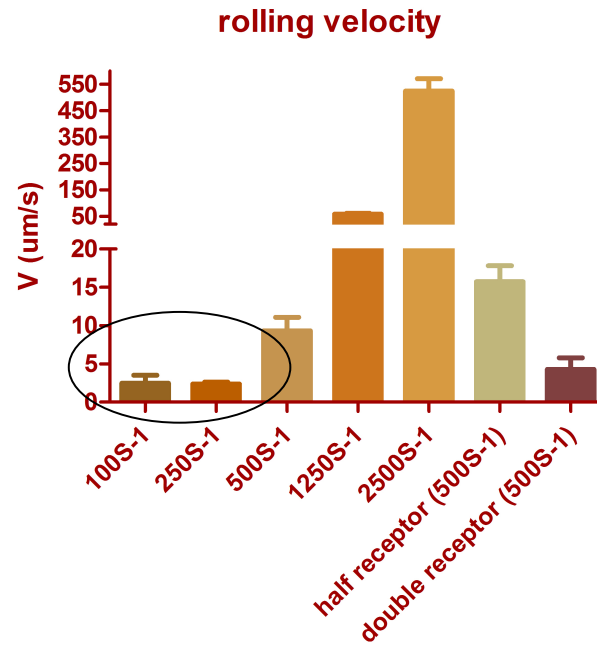
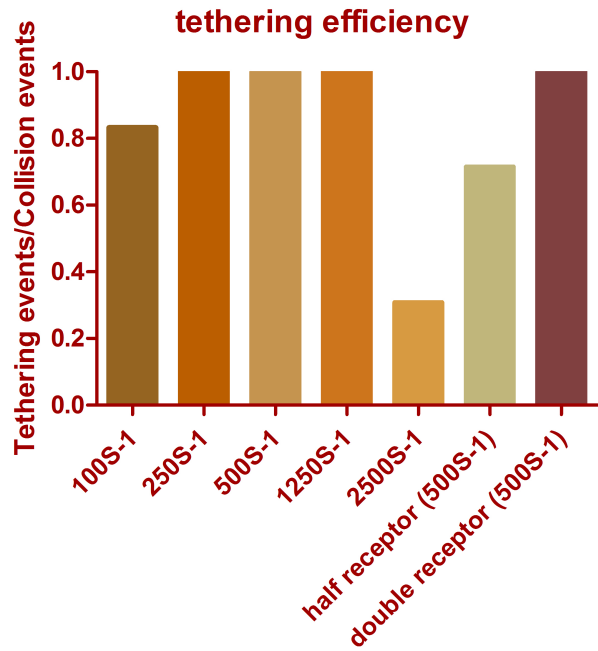
Platelet Size:  $1 \mu\text{m} \times 1 \mu\text{m} \times 0.25 \mu\text{m}$   
 Surface receptor density:  $\sim 1500/\mu\text{m}^2$   
 $K_r^0: 5.47 \text{ S}^{-1}$   
 Other parameters see: NA Mody, et al. Biophysical Journal, Vol. 95 Sep. 2008



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# Single Platelet: Rolling









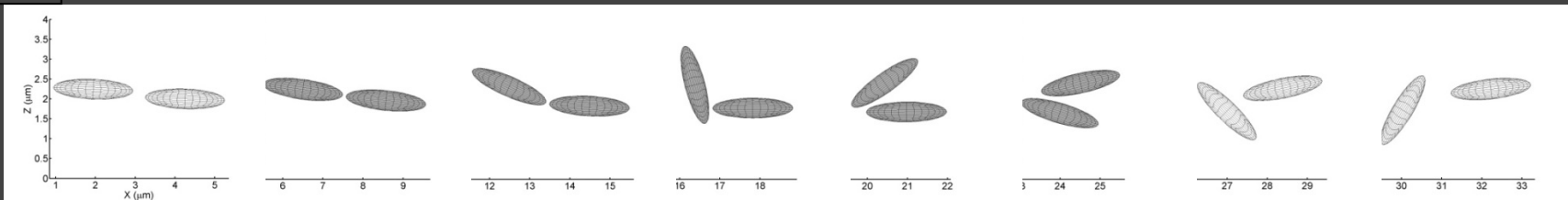
# Cornell University Two Platelets: Collision in Flow

Both near-wall and far-wall platelet collision events have identical initial configurations:  $DX = 2.5 \text{ mm}$ ;  $DZ = 0.25 \text{ mm}$  between centroids.

**A**

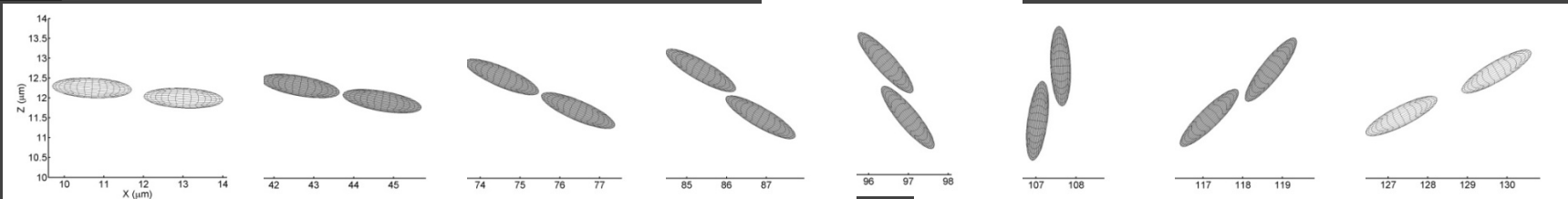
## CLOSE TO WALL

Mody and King, Part I, Biophys. J. 2008



**B**

## FAR FROM WALL



**A**

## CLOSE TO WALL

- Contact Time  $T_c = 22.84 \text{ ms}$
- Max (Instantaneous Contact Area  $A_c$ ) =  
Platelet 1:  $1.27 \text{ } \mu\text{m}^2$ ; Platelet 2:  $1.26 \text{ } \mu\text{m}^2$

$$\int_0^{T_c} A_c^{\text{platelet}} dt = 9.7 \text{ } \mu\text{m}^2\text{-ms Platelet 1}$$

$$= 10.0 \text{ } \mu\text{m}^2\text{-ms Platelet 2}$$

**B**

## FAR FROM WALL

- Contact Time  $T_c = 17.39 \text{ ms}$
- Max (Instantaneous Contact Area  $A_c$ ) =  
Platelet 1:  $0.8 \text{ } \mu\text{m}^2$ ; Platelet 2:  $0.85 \text{ } \mu\text{m}^2$

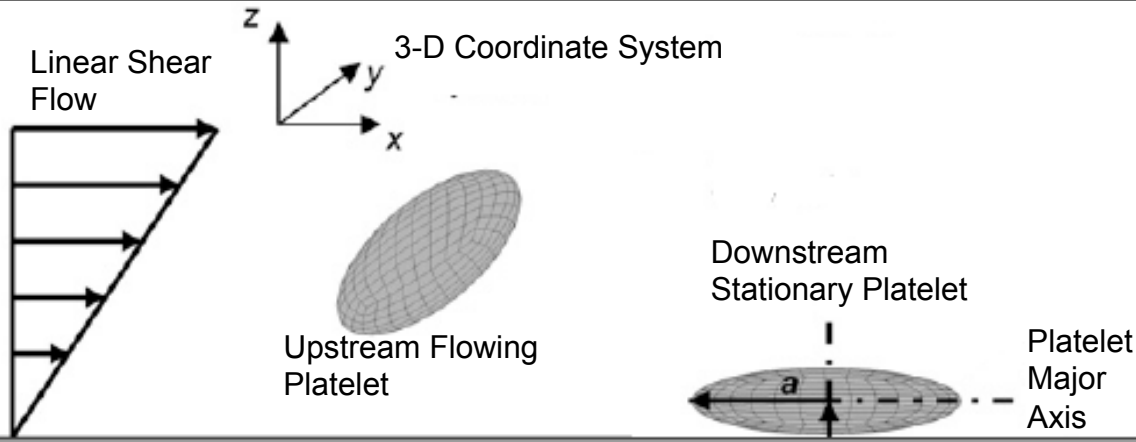
$$\int_0^{T_c} A_c^{\text{platelet}} dt = 6.0 \text{ } \mu\text{m}^2\text{-ms Platelet 1}$$

$$= 6.1 \text{ } \mu\text{m}^2\text{-ms Platelet 2}$$

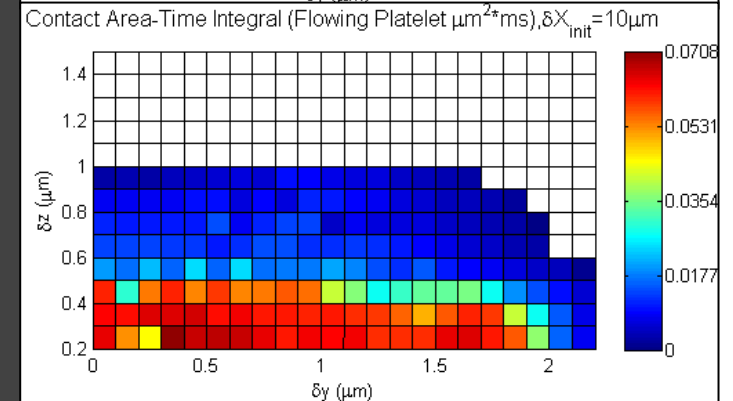
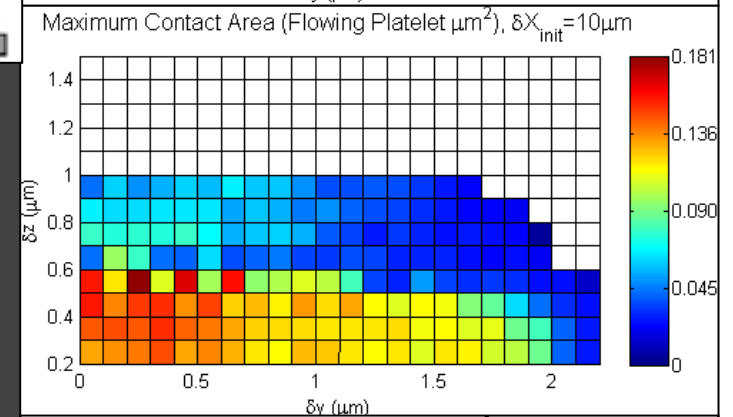
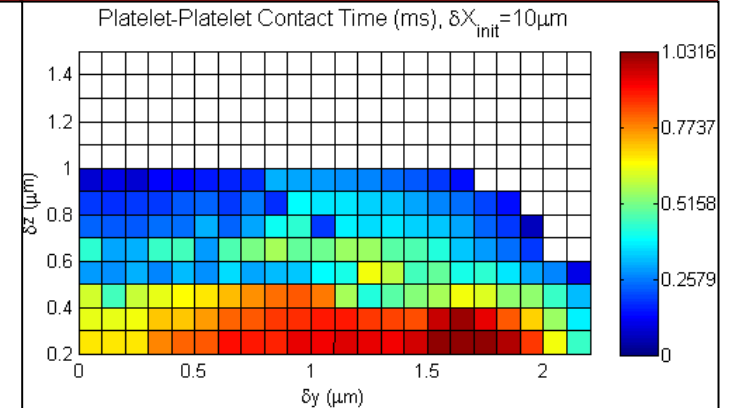
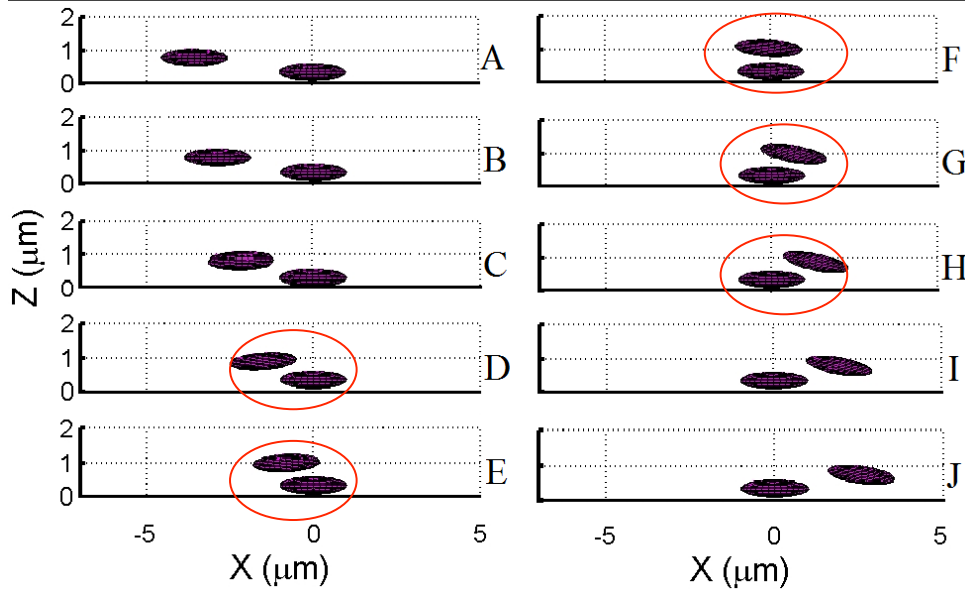


Cornell University

# Two Platelets: the beginnings of aggregation



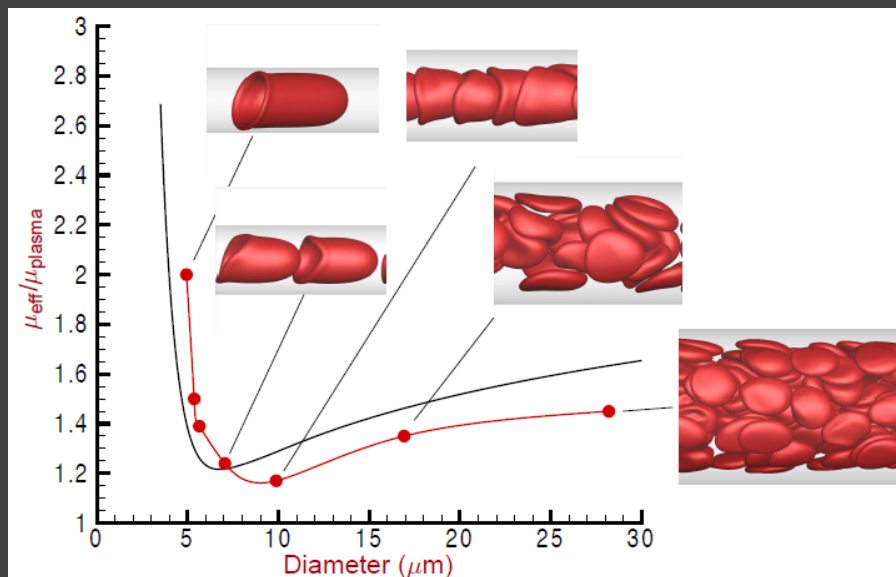
Contact: when closest distance  $< 0.128\mu\text{m}$   
(trimolecular bond length)



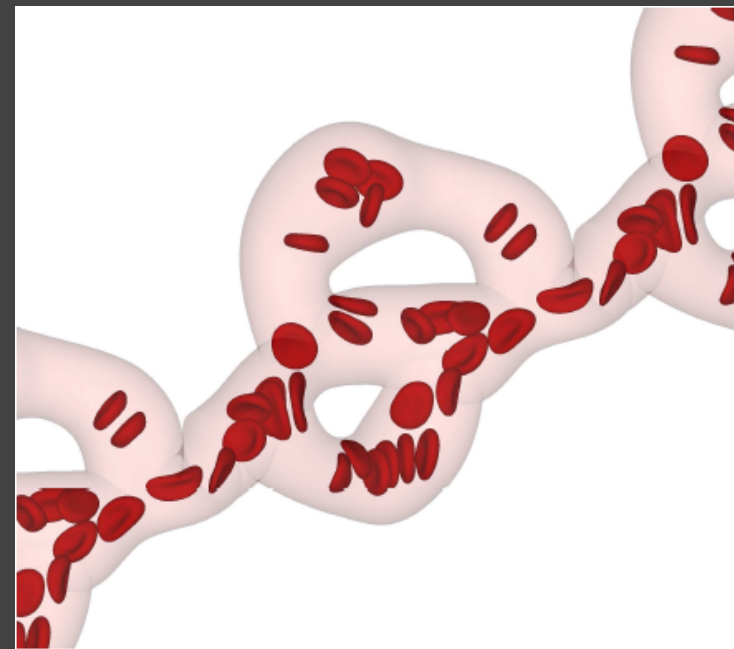


A spectral surface integral methods developed for solving the viscous flow, and the motion of the massless membrane:

- Fast: an  $O(N \log N)$  particle-mesh Ewald (PME) approach
- handle **deformable** RBCs
- deals with a **large number** of cells
- deal with **complicated** vessel geometry



Effective viscosity at Hct=30%

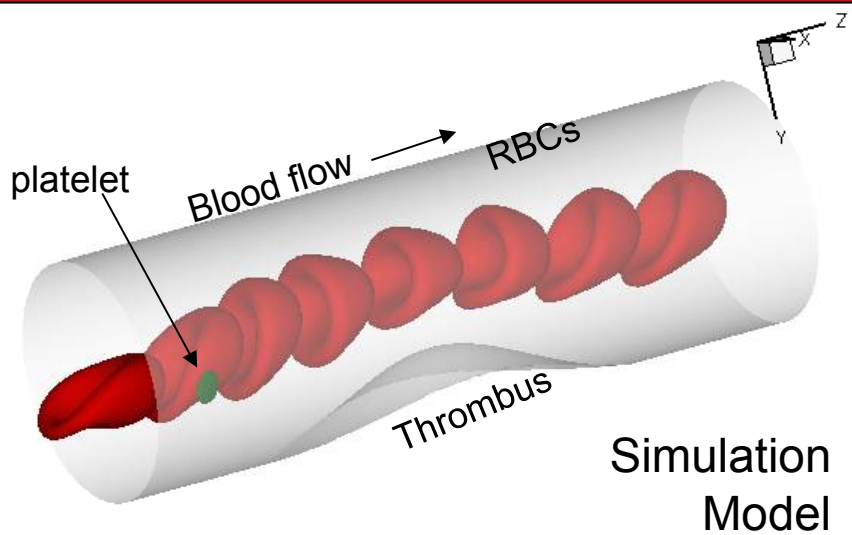


Blood flow through complex network

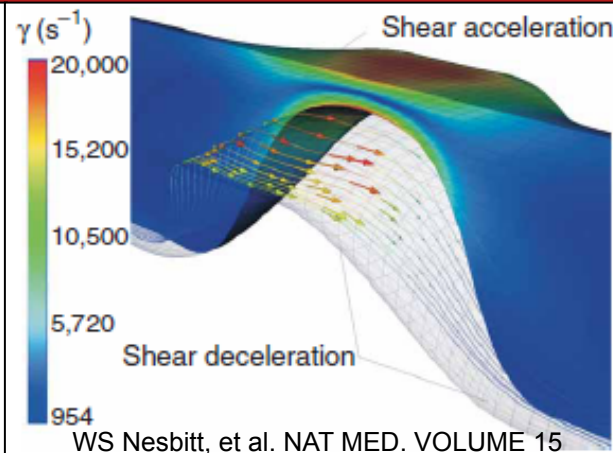


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# Clumps of Platelets: Micro Thrombi

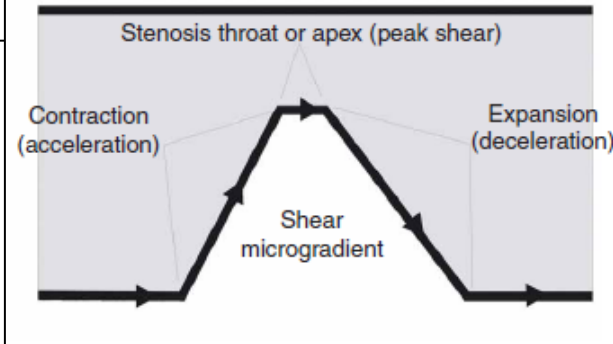
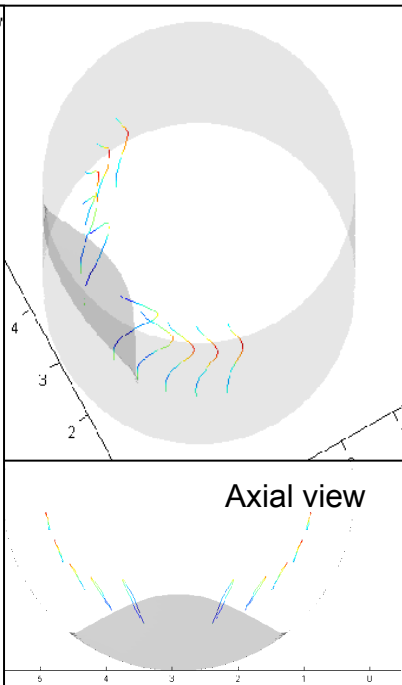
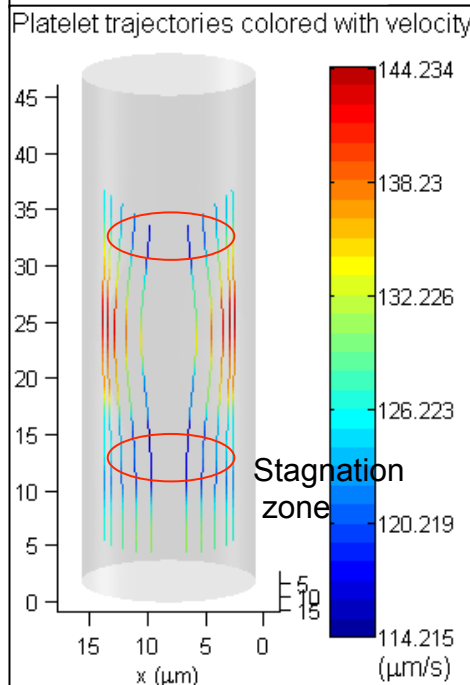


Simulation Model

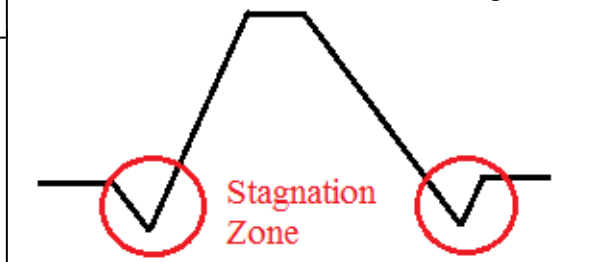


WS Nesbitt, et al. NAT MED. VOLUME 15 [ NUMBER 6 [ JUNE 2009

“A shear gradient–dependent platelet aggregation mechanism drives thrombus formation”—  
WS Nesbitt, et al. NATURE MEDICINE. VOLUME 15 NUMBER 6 JUNE 2009



We propose: the existence of stagnation zone further increases the shear gradient



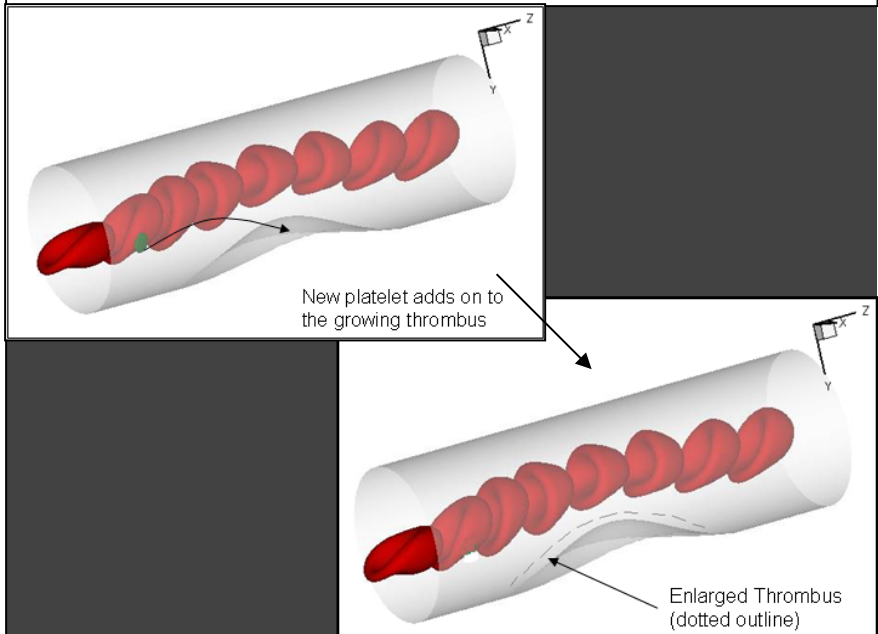
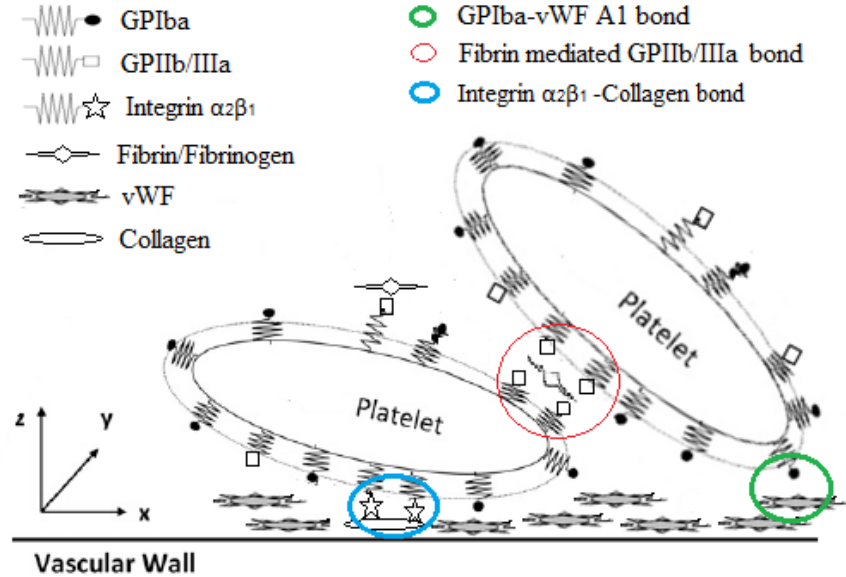
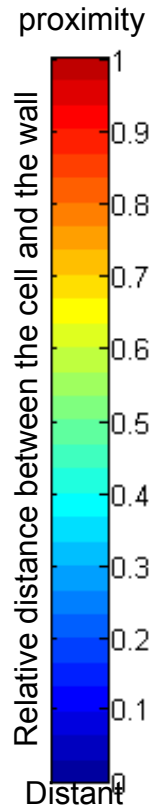
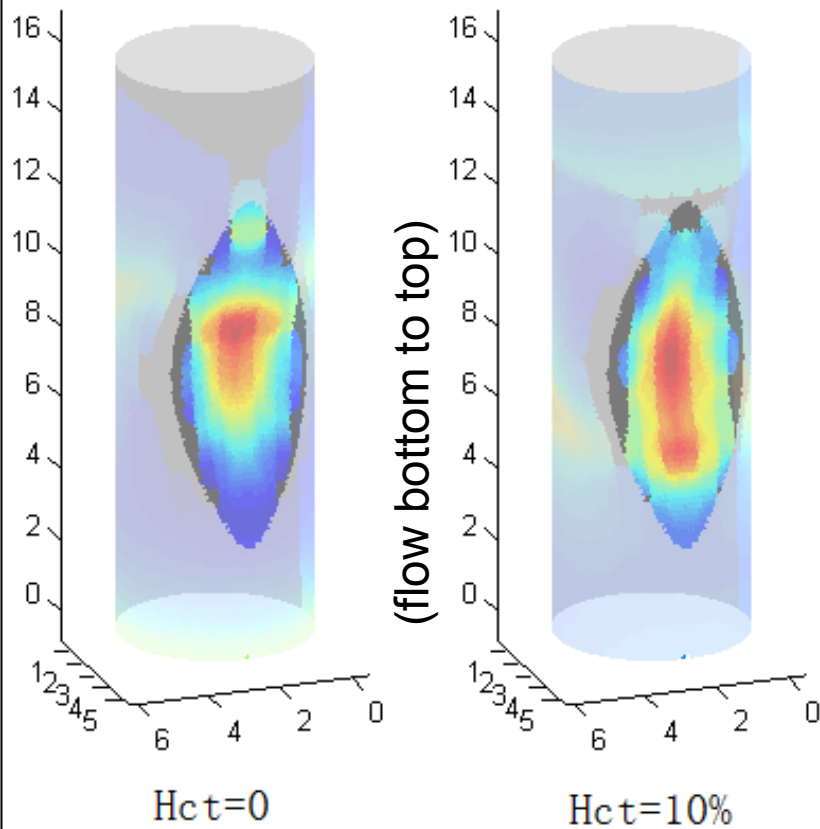


RBCs enhance platelets deposition.

Thrombus Growth Model



### Platelet Deposition Potential Map



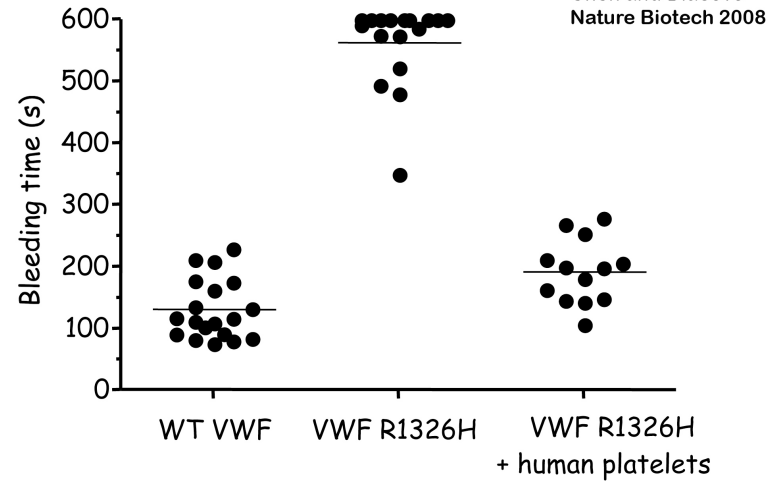


VWF R<sup>1326</sup>H mice



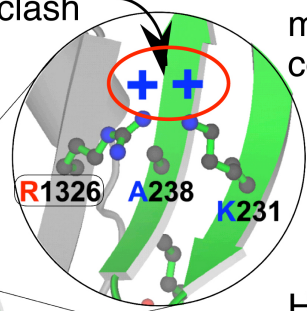
Inject fluorescent human platelets

pulsed nitrogen dye laser  
↓  
Test thrombus formation

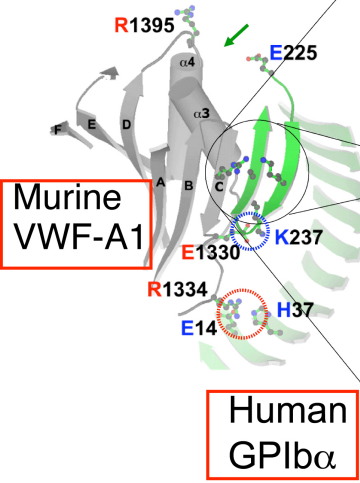
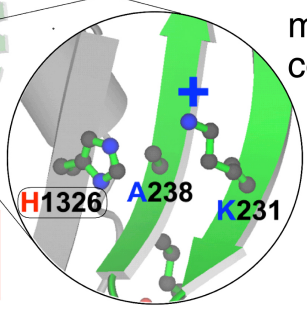


electrostatic clash

Human GPIb $\alpha$  – mouse VWF-A1 complex

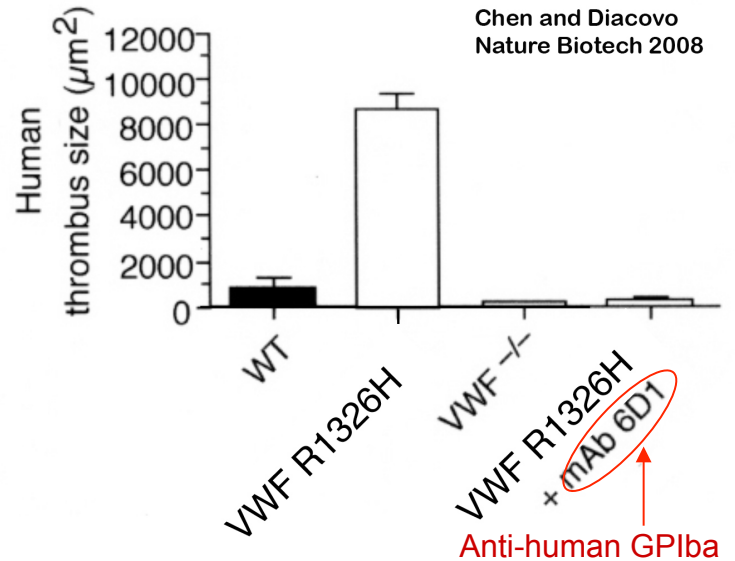


Human GPIb $\alpha$  – mutant murine VWF-A1 complex



Chen and Diacovo Nature Biotech 2008

## Human platelets in mice



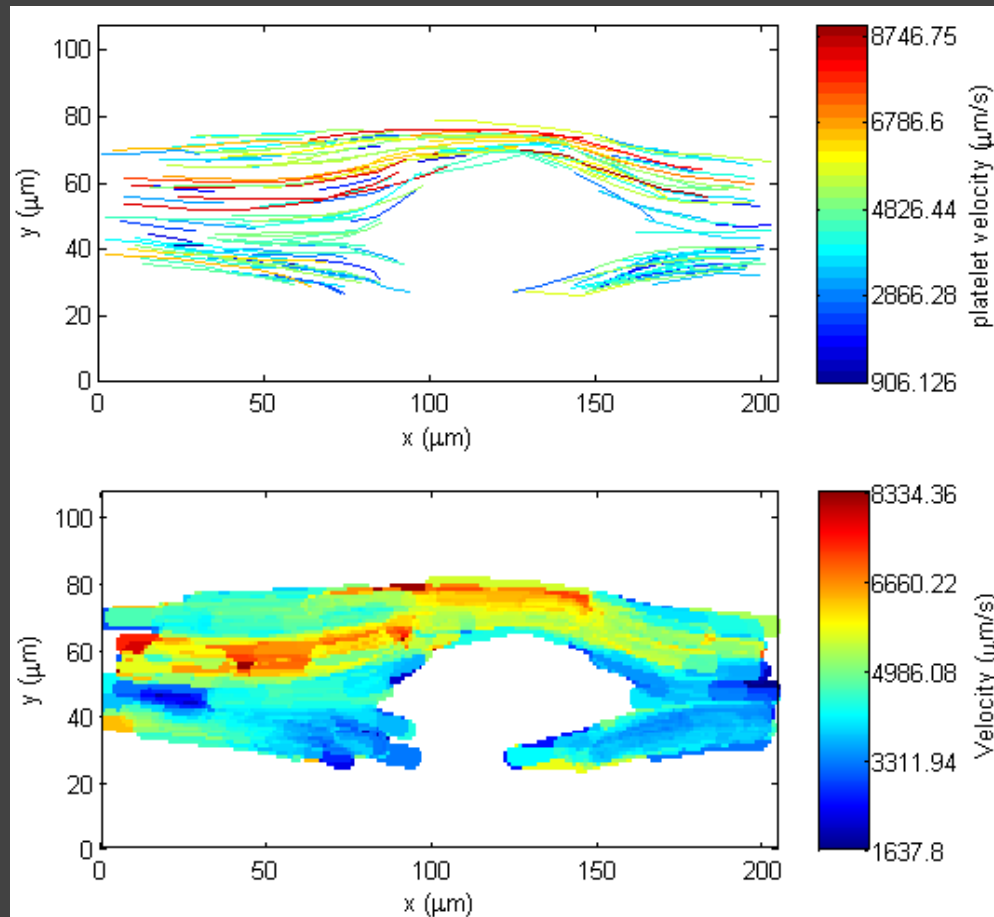
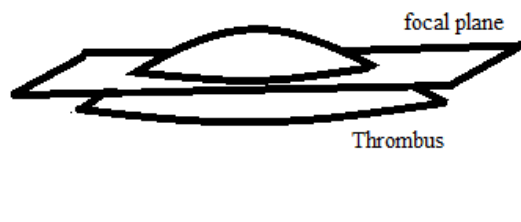
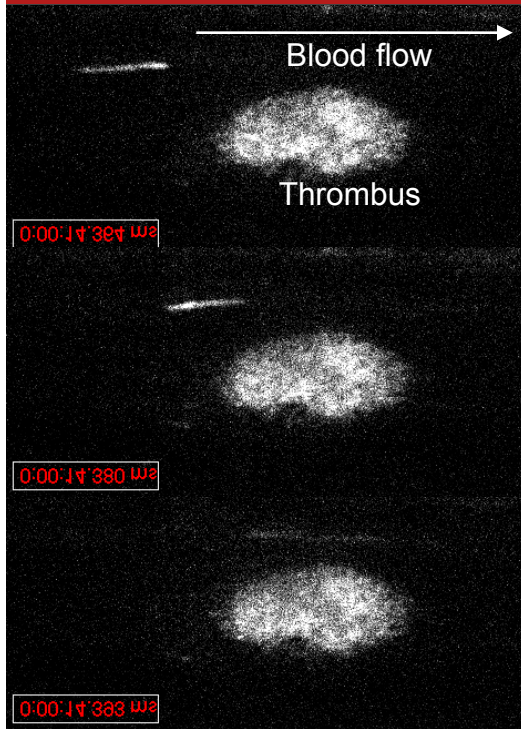


# Platelet Flow past a growing Thrombus

Digital analysis of platelet flow around a platelet-rich thrombus in vivo. (~400 frames, 6s real time)

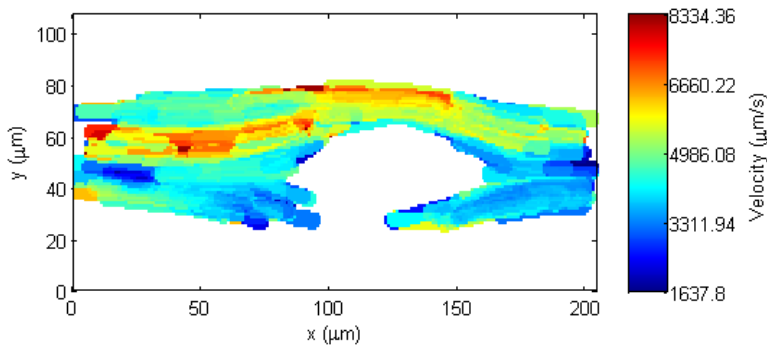
*Up*: cell trajectories color coded for velocity magnitude.

*Down*: 2-D color map of velocity magnitude.





# Detecting Thrombus Shape Change

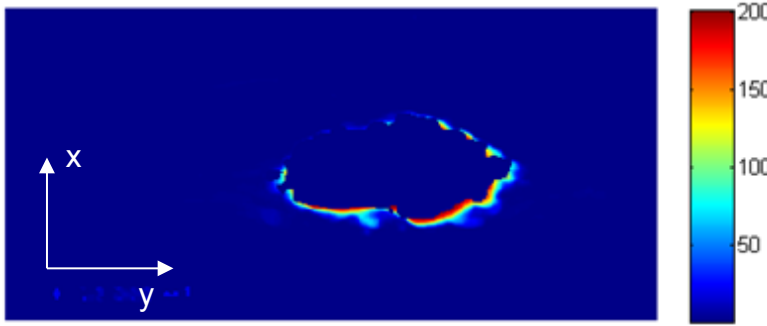


Thrombus tend to **shrink** at surface with **high shear stress** and **extend** at surface with **low shear stress** where platelet is more easy to tether.

Thombus shift is not caused by pulmonary effect. (400

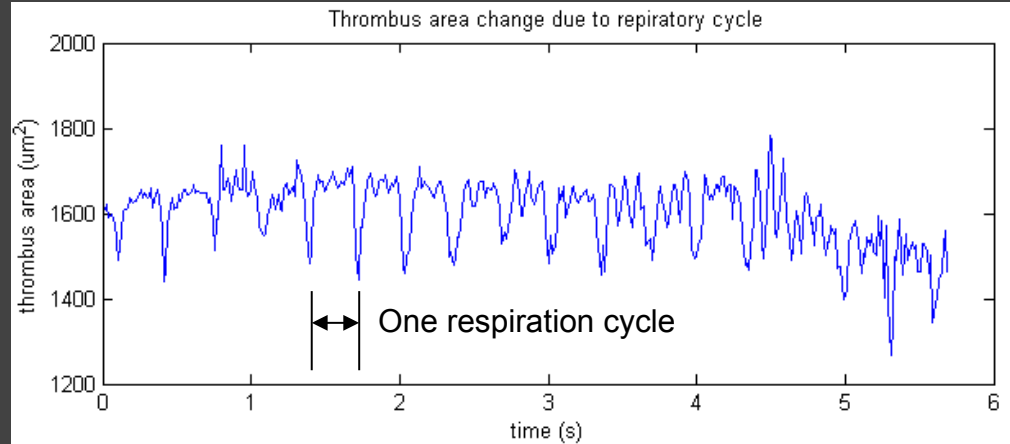
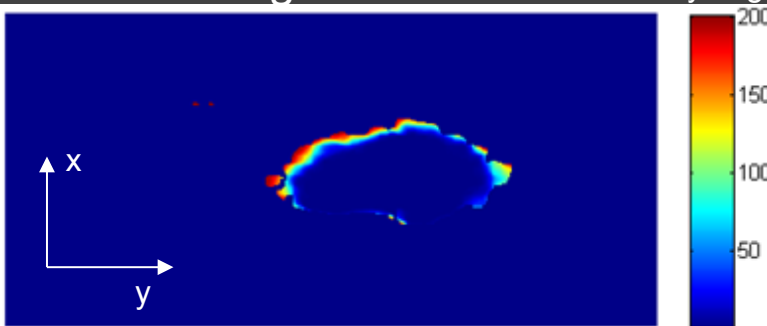
Growing area

Most early growth

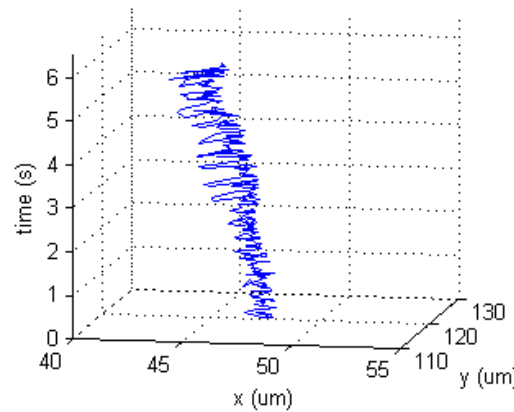


Degrade area

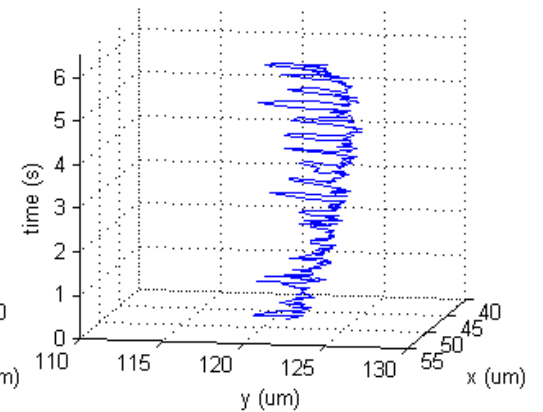
Most early degraded



Thrombus center shift



Thrombus center shift







**Platelet Adhesive Dynamics:**

- Flow characteristics of platelet shaped cells
- Characterizing particle-particle collision phenomena
- Dynamics of GPIIb/IIIa-A1 mediated platelet-vessel tethering/rolling, initiation of thrombosis.

The **existence of “stagnation zones”** both upstream and downstream the thrombus enhances the shear-gradient dependent thrombus formation

**RBCs enhance platelet deposition**, which leads to enhancement of thrombus growth.

**Characterizing the flow pattern** around a human thrombus in vivo.

**Explore the thrombus shifts** towards low shear stress region.

***Funded by NIH Grant No. HL097971***